

Original Research

Effect of Footwear Versus Barefoot on Double-Leg Jump-Landing and Jump Height Measures: A Randomized Cross-Over Study

Kim Hébert-Losier¹^a, Caleb Boswell-Smith¹, Ivana Hanzlíková²¹ Te Huataki Waiora School of Health, University of Waikato, ² Department of Physiotherapy, Palacký University Olomouc

Keywords: Anterior Cruciate Ligament, biomechanics, knee, screening

<https://doi.org/10.26603/001c.81107>

International Journal of Sports Physical Therapy

Vol. 18, Issue 4, 2023

Background

Assessing individuals in their own athletic footwear in clinics is common, but can affect movement, performance, and clinical measures.

Purpose

The aim was to compare overall Landing Error Scoring System (LESS) scores, injury risk categorization, specific LESS errors, and jump heights between habitual athletic footwear and barefoot conditions.

Study design

Randomized cross-over laboratory study.

Methods

Eighty healthy individuals (55% male) completed the LESS following standard procedures (i.e., land from a 30-cm box to a distance of 50% of body height and then jump upwards maximally). Participants performed the LESS three times in two randomized conditions: footwear and barefoot. LESS data were extracted from 2D videos to compare group-level mean LESS scores, group-level and individual-level injury risk categorization (5-error threshold), specific landing errors, and jump heights between conditions.

Results

LESS scores were significantly greater (0.3 errors, $p=0.022$) and jump heights were significantly lower (0.6 cm, $p=0.029$) in footwear than barefoot, but differences were *trivial* ($d = 0.18$ and -0.07 , respectively) and not clinically meaningful. Although the number of high injury-risk participants was not statistically different at a group level ($p=1.000$); 27 individuals (33.8%) exhibited a clinically meaningful difference between conditions of one error or more in LESS score, categorization was inconsistent for 16.3% of individuals, and four of the 17 landing errors significantly differed between conditions.

Conclusion

At a group level, habitual athletic footwear does not meaningfully influence LESS scores, risk categorization, or jump height. At an individual level, footwear can meaningfully affect LESS scores, risk categorization, and alter landing strategies. Use of consistent protocol and footwear is advised for assessing movement patterns and injury risk from the LESS given the unknown predictive value of this test barefoot.

Level of Evidence

Level 3.

^a Corresponding Author:

Kim Hébert-Losier

University of Waikato, Adams Centre for High Performance, 52 Miro Street, 3116 Tauranga, New Zealand

E-mail: kim.hebert-losier@waikato.ac.nz, telephone: +64 7 837 9476, fax: +64 7 838 4504

INTRODUCTION

Anterior cruciate ligament (ACL) injury is one of the most common sport injuries and has a devastating influence on the activity levels and quality of life of individuals.¹ ACL injuries can occur without physical contact, and thus, are considered preventable.² The most common situation for noncontact ACL injuries appears to be deceleration, which is when the athlete cuts, changes direction, or lands from a jump.³ The Landing Error Scoring System (LESS) is a screening tool used to identify athletes presenting with high injury-risk movement patterns during a double-leg jump-landing (DLJL) task.⁴ Clinicians score 17 items based on movements during the DLJL task. The overall LESS score ranges from 0 to 17 errors where lower scores reflect fewer landing errors and thus fewer movement patterns linked with noncontact ACL injuries. Scores of five or more errors indicate poor jump-landing technique⁴ and have been linked to higher risk of ACL injury.⁵ Specifically, the risk ratio for sustaining a noncontact or indirect contact ACL injury was 10.7 in individuals scoring five errors or more compared to less than five errors.⁵ Compared to healthy controls, LESS scores are greater after an unilateral ACL reconstruction despite being cleared to return to physical activity, indicating that the LESS may provide useful information to guide rehabilitation and return-to-sport decisions.⁶

Across the literature, the overall LESS score demonstrates good-to-excellent reliability, and moderate-to-excellent validity versus 3-dimensional (3D) motion capture data for the items linked with risk factors for knee injury.⁷ Overall LESS scores are, however, sensitive to various factors, such as gender, previous injury, and intervention programs.⁸ Research has also identified that jump landing distance⁹ and final LESS score computational method¹⁰ can affect LESS scores and individual-level risk categorization. Altogether, these studies highlight that several factors and procedural methods need to be considered when administering and interpreting LESS outcomes.

Footwear plays a central role in sport and is typically designed to enhance performance and protect the body from injury. However, footwear can influence the human-ground interaction and result in different multi-joint landing strategies to moderate impact forces.¹¹ Indeed, initial contact from a 30-cm DLJL task similar to the LESS has been associated with a more plantar-flexed ankle,¹² greater foot-ground angle,¹² and smaller knee range of motion¹³ when performed barefoot compared to with shoes. Together, these studies indicate that LESS scoring might differ between barefoot and footwear conditions, although this topic has not yet been explicitly examined. Although the LESS is traditionally performed wearing a person's own athletic shoes,^{6,10} it has also been conducted barefoot.¹⁴ Therefore, the aim was to compare overall LESS scores, injury risk categorization, and specific LESS errors between habitual athletic footwear and barefoot conditions. The hypothesis was that wearing footwear would result in higher overall LESS scores, lead to a greater number of individuals classified at high risk of injuries, and influence specific LESS errors compared to barefoot. Given how footwear can

influence jump performance,¹⁵ jump heights from flight times were also compared between conditions.

MATERIALS AND METHODS

EXPERIMENTAL APPROACH

A randomized cross-over experimental design was used to explore the influence of footwear on LESS scores, LESS injury risk categorization, specific LESS errors, and jump height. Sample size calculations were performed *a priori* using G*Power 3.1.9.7, and applied a standard two-tailed hypothesis, 90% power ($\beta = 0.10$), 5% significance level ($\alpha = 0.05$), one error LESS difference in paired means defining a clinically-meaningful change,^{4,8} and 2.47 standard deviation of the difference in paired means based on previous work implementing similar testing procedures and comparing LESS scores between two experimental conditions.⁹ Based on these assumptions, 67 participants were required and would be sufficient to detect a *small* effect size difference (Cohen $d = 0.40$) between conditions. A sample size of 80 participants was targeted to account for a 20% drop out rate.

PARTICIPANTS

Eighty participants were recruited and tested within one month in 2021 from a convenience sample of healthy university students. All volunteers were free of injury, illness, or conditions that may have affected their movements or landing mechanics. Participants with a lower extremity, back, or pelvis injury in the prior three months were excluded. LESS testing was performed in individuals' own athletic footwear, as is typical in research and clinical settings.^{6,10} Participants were excluded when their footwear scored 70% or more on the Minimalist Index¹⁶ (described under *Procedures*) as deemed to represent minimal shoes¹⁷ that could potentially mimic barefoot.¹⁸ It was deemed inappropriate to merge data from trials performed in conventional athletic footwear to those from minimal footwear given the reported effect of these different footwear types on the biomechanics of dynamic tasks.¹⁸⁻²⁰ All participants signed an informed consent document that explained the potential risks of participation (e.g., chance of injury due to physical activity). The University of Waikato Human Research Ethics Committee (HREC(Health)#2017-41) approved the protocol before data collection, which adhered to the Declaration of Helsinki. This project was retrospectively registered with the Australian New Zealand Clinical Trials Registry (ACTRN12622001358730).

PROCEDURES

Following informed consent, baseline characteristics of participants were collected, which included measuring body height using a stadiometer (seca model 0123, Medical Measuring Systems and Scales, Mount Pleasant, South Carolina) and mass on an electronic scale (seca model ESE813, Medical Measuring Systems and Scales, Mount Pleasant, South Carolina). Participants also completed a short sport

participation questionnaire, as well as the self-administered short-form International Physical Activity Questionnaire.²¹ According to their responses to the latter, participants were categorized as having high, moderate, or low physical activity levels.²¹ Participants were pre-informed of the study aims and asked to bring their own athletic footwear for testing. Footwear characteristics were measured for all participants and included the use of the Minimalist Index¹⁶ alongside more traditional characteristics. In summary, the Minimal Index measures five shoe features to quantify the level of minimalism of footwear, where 100% represents the highest degree of minimalism. The five characteristics are footwear mass, longitudinal and torsional flexibility, stack height, heel-to-toe drop, and the presence/absence of technologies. Minimal Index scores of participants' own shoes ranged from 4 to 64%. The hardness of the midsole material in the center of the heel region was assessed using an Asker-C durometer (Supertech Precision Supply Co., LTD, Osaka, Japan) with an accuracy of 1 unit. The average of three consecutive durometer measurements was recorded and used to quantify Asker-C heel hardness.

All experimentation took place in a biomechanics laboratory. The original LESS testing and scoring procedures were used,⁴ except in the barefoot condition when no shoes were worn. Participants jumped horizontally from a 30-cm box to 50% of their body height and jumped vertically as high as possible upon landing. The horizontal landing distance was indicated on the floor using tape. Trials were disregarded when participants did not land at 50% of their body height or did not perform the task in one fluid motion. Feedback on performance was not given to avoid influencing outcomes²² unless the task was performed inappropriately. Before the formal tests, participants were allowed up to three familiarization trials in both the footwear and barefoot conditions immediately before testing for each corresponding condition. For testing, each participant performed three trials in each condition with 30 seconds rest between trials and 15 minutes rest between conditions. The order of conditions was block randomized prior to study commencement by a third party to ensure an equal number of participants starting in each condition. The condition tested first (barefoot or footwear) was allocated sequentially and announced to participants upon study enrollment. It was not possible to blind the participants and examiners to the condition examined.

Two cameras with a focal length of 8.8 to 73.3 mm (35-mm equivalent focal length of 24-200 mm) captured the DLJL trials at 120 frames per second (Sony RX10 II, Sony Corporation, Tokyo, Japan). These videos were used to derive LESS scores post testing. One camera captured frontal plane movement and the other captured right-side sagittal plane movement. Each camera was placed 3.5 meters away from the landing area and mounted on tripods with a 1.3 m lens-to-ground distance. The videos were analyzed using Kinovea (version 0.9.4, www.kinovea.org). The time from take-off from the ground to the final landing was extracted from the sagittal plane videos to compute jump heights from flight times as²³:

$$h = \frac{1}{8} \cdot g \cdot t^2 \cdot 100 \quad (1)$$

where h is jump height (cm), g is gravitational acceleration constant (9.81 m/s²), and t is flight time (s).

DATA PROCESSING

A single rater (CBS) with over three years of experience analyzing human movement conducted all data processing after receiving four training sessions from an expert LESS rater (IH) who had completed over 400 LESS evaluations. The single rater completed more than 20 LESS assessments before analyzing the current dataset. After analyzing all videos for this study (i.e., 80 participants x 3 trials x 2 conditions = 480 videos), the rater re-analyzed the first 20 to ensure consistency in ratings. The rater was blinded to the randomization sequence and LESS scores of individuals from the other experimental condition, as trials were presented in a random order for rating.

To ensure rater reliability of the videos collected, two raters (CBS and DB) with similar experience and LESS training participated in an inter-rater and intra-rater reliability study of the overall LESS score using a subset of videos from 10 participants. Inter-rater reliability was excellent based on intra-class correlation coefficient (ICC) and 95% confidence interval [lower, upper] values for both footwear (ICC_(2,1) = 0.957 [0.815, 0.990]) and barefoot (ICC_(2,1) = 0.957 [0.847, 0.989]) conditions. Intra-rater reliability was also excellent for both footwear (ICC_(3,1) = 0.974 [0.903, 0.993]) and barefoot (ICC_(3,1) = 0.970 [0.815, 0.993]) conditions.

STATISTICAL ANALYSIS

The effect of footwear on group mean LESS scores, injury risk categorization (high risk, LESS ≥ 5 errors; low risk, LESS < 5 errors), individual-level risk categorization, and jump height was examined. The average of participants' three trials was used for analysis. Taking the average of three trials is consistent with the original LESS protocol⁴ and is the most common approach used to interpret LESS data.¹⁰ Differences in group mean LESS scores and jump heights between conditions were assessed using mean differences, two tailed paired t -tests, and Cohen's d effect sizes for paired samples using an average variance with 95% confidence intervals. Cohen's d effect sizes were considered *small*, *medium*, and *large* when reaching 0.20, 0.50, and 0.80, respectively, and *trivial* when less than 0.20.²⁴

Differences in the number of participants categorized at high and low risk of injury based on the 5-error LESS threshold between conditions were assessed using McNemar's tests and odds ratio with 95% confidence intervals. The odds ratio reflects the number of participants exclusively at high risk in the footwear condition versus those exclusively at high risk in the barefoot condition. Hence, odds ratios > 1.0 reflect a higher proportion of at-risk individuals in the footwear condition. The number of participants demonstrating a clinically meaningful change in LESS scores (i.e., one error or more difference)^{4,8} between conditions was also examined. Finally, differences in the

Table 1. Demographic characteristics of participants. Data are presented as means \pm standard deviations or counts.

Characteristics	Males (n = 44)	Females (n = 36)	Both (n = 80)
Participants			
Age (y)	20.1 \pm 2.0*	19.9 \pm 2.6*	20.0 \pm 2.3†
Height (cm)	180.5 \pm 7.0	168.4 \pm 6.6	175.0 \pm 9.1
Mass (kg)	84.1 \pm 19.3	68.8 \pm 10.2	77.1 \pm 17.6
BMI (kg/m ²)	25.9 \pm 6.8	24.2 \pm 3.2	25.1 \pm 5.5
IPAQ (high:mod:low)	34:8:1*	22:11:1†	56:19:2‡
Sport (field or court:other:none)	30:13:0*	12:21:2*	42:34:2†
Footwear			
Mass (g)	329.8 \pm 70.2	305.2 \pm 66.1	318.8 \pm 69.5
Stack height (mm)	25.5 \pm 8.0	24.6 \pm 6.5	25.1 \pm 7.4
Forefoot height (mm)	14.7 \pm 4.4	15.4 \pm 4.7	15.0 \pm 4.5
Heel-to-toe drop (mm)	10.8 \pm 5.8	9.2 \pm 4.5	10.1 \pm 5.3
Minimalist Index (%)	30.9 \pm 18.1	31.1 \pm 16.1	30.9 \pm 17.3
Asker-C heel hardness (a.u.)	35.4 \pm 7.7	38.4 \pm 6.2	36.8 \pm 7.2

Notes. *Missing data from one participant. †Missing data from two participants. ‡Missing data from three participants. a.u., arbitrary units; BMI, body mass index; IPAQ, International Physical Activity Questionnaire; mod, moderate.

occurrence of specific LESS errors between conditions were explored using McNemar's tests. For each participant, an error was considered present when present in two of the three trials for Items 1-15. For Items 16-17, an error was considered present when the 'average' rating was present in two of three trials or when the 'poor/stiff' rating was present in one of three trials.^{4,9} The significance level was set at $p \leq 0.05$ for all analyses, which were conducted using Microsoft Excel for Microsoft 365 MSO (version 2109, Microsoft Corp, Redmond, WA, USA) and RStudio® version 1.1.463 with R version 4.0.5 (R Core Team, 2021). There were no missing data, and all participants completed the experimentation without harm.

RESULTS

Eighty participants (44 males and 36 females) completed the study. Their demographic and footwear characteristics are presented in [Table 1](#). Approximately half of participants (52.5%) participated in court or field sports (e.g., basketball, football, netball, rugby), with most of the others (42.5%) participating in another sporting activity (e.g., running, cycling, rowing).

The group mean LESS scores in the footwear condition (range: 2.7-10.0 errors) was significantly greater (0.3 errors, $p=0.022$) than barefoot (range: 2.3-10.0 errors), as shown in [Table 2](#). However, the magnitude of the difference was *trivial* (Cohen $d=0.18$ [0.03, 0.33]). The number of individuals classified at high risk was not significantly different between conditions (62 participants footwear vs 61 participants barefoot, $p=1.000$), with seven participants categorized at high risk exclusively in footwear and six barefoot ([Figure 1](#)). At an individual level, 27 participants (33.8%) demonstrated a clinically meaningful difference of one error or more in LESS scores between conditions. The risk

categorization was conflicting between conditions for 13 participants (16.3%, [Figure 2](#)). Six participants changed from being categorized as low risk in footwear to high risk barefoot, and seven from high risk in footwear to low risk barefoot. The difference in mean LESS score was one or more in all but one of these participants (92.3%). Jump height in footwear (range: 8.5-56.4 cm) was significantly lower (-0.6 cm, $p=0.029$) than barefoot (range: 11.4-55.1 cm), but the difference was *trivial* ($d = -0.07$ [-0.13, -0.01], [Table 2](#)).

The occurrence of specific LESS errors significantly differed between conditions for four of the 17 items. Specifically, there were more errors for Item 4 (ankle plantar flexion at initial contact) and Item 5 (knee valgus at initial contact) in footwear, and more errors for Item 8 (stance width-narrow) and Item 10 (foot position-toe out) barefoot ([Table 3](#)).

DISCUSSION

In agreement with the hypothesis, footwear led to significantly higher LESS scores than barefoot; however, the difference was *trivial* and not clinically meaningful as it was less than one error.^{4,8} Footwear led to significantly lower jump heights than barefoot, but the difference was also *trivial* and not clinically meaningful as it was less than the 2 cm typical error associated with this measure.²⁵ A greater number of participants at high risk of injury when wearing footwear was hypothesized; however, the number of high injury-risk participants was not significantly different to barefoot. Despite the similarities in LESS scores and high injury-risk categorization at a group level, differences in LESS scores were clinically meaningful (i.e., one error or more) for approximately one third of participants, and individual-level risk categorization was incon-

Table 2. Comparison of Landing Error Scoring System (LESS) mean scores and group-level injury risk categorization between footwear and barefoot conditions. Data are reported as means \pm standard deviations and differences with 95% confidence intervals [lower, upper].

Outcome	Footwear	Barefoot	Difference	p-value
LESS score (errors)	6.2 \pm 1.5	5.9 \pm 1.6	0.3 [0.05 to 0.52]	0.022^{*†}
High injury risk (%)	77.5%	76.3%	1.17 [0.39 to 3.47]	1.000 [‡]
Jump height (cm)	32.1 \pm 9.2	32.8 \pm 8.9	-0.6 [-0.1, -1.2]	0.029^{*†}

Note. ^{*}Significant difference between conditions ($p \leq 0.05$) are in bold. [†] Difference in means with paired t -test. [‡] Odds ratio significance with McNemar's test.

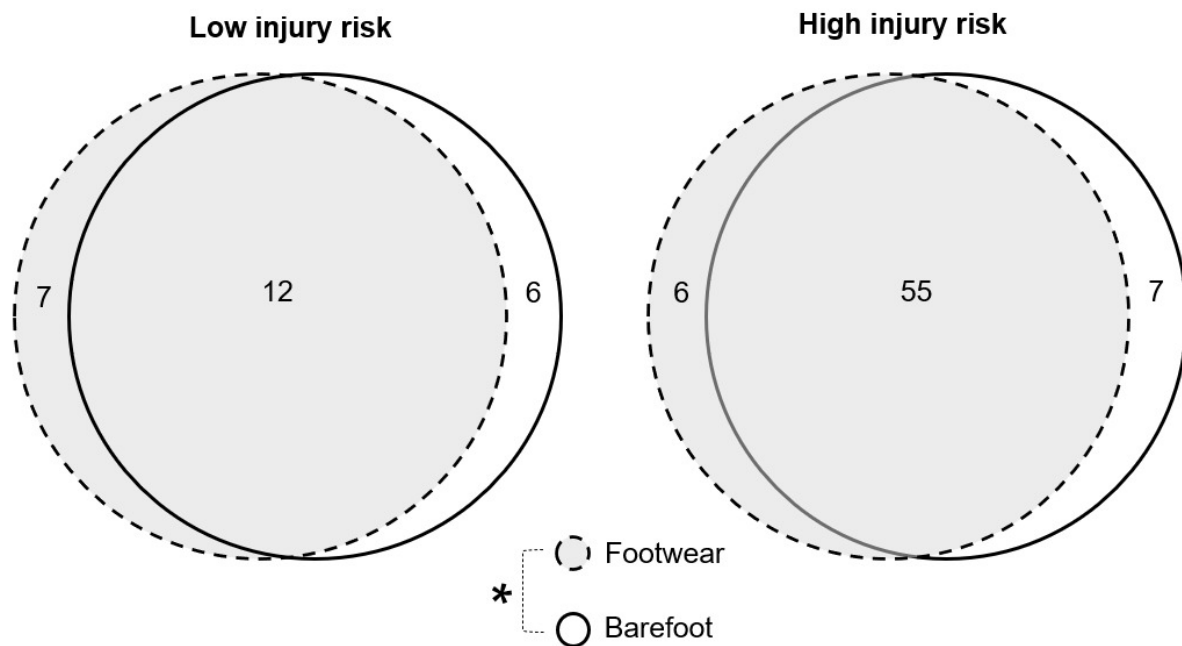


Figure 1. Venn diagrams representing participants at high (≥ 5 errors) and low (< 5 errors) injury risk for both footwear and barefoot conditions. The number in the circle represents the sum of participants categorized at low or high risk for each condition. The overlapping area represents the number of participants at low or high risk in both conditions. ^{*}Significant difference in the proportion of individuals at high and low risk based on McNemar's tests ($p \leq 0.05$).

sistent for approximately a sixth of participants between conditions. Furthermore, differences in specific landing errors were noted, with greater odds of knee valgus and heel-to-toe or flat foot landing at initial contact in footwear, and lesser odds of landing with a narrow stance width and toe-out foot position. Overall, performing the LESS with compared to without footwear led to comparable mean LESS scores, group-level injury risk categorization, and jump heights, but influenced specific LESS errors, individual-level risk categorization (i.e., 16.3% of individuals inconsistently categorized between conditions), and LESS scores of some participants in a clinically meaningful manner (i.e., change of one error or more for 33.8% of individuals).

The mean LESS scores in footwear in this study are similar to means reported elsewhere for similar cohorts of young active individuals.^{9,10} The current findings also reflect previous ones where altering the jump landing distance of the LESS did not meaningfully affect group-level LESS scores and risk categorization, but significantly influ-

enced the odds of individual LESS errors and individual-level injury risk categorization.⁹ The comparable outcomes imply that studies can implement the LESS either with shoes or barefoot when the main outcome is the group mean LESS score or group-level injury risk categorization. Implementing the LESS barefoot can be easier to standardize across participants as guarantees no effect of footwear or footwear type on landing mechanics. Nonetheless, it would be inappropriate to compare specific LESS errors between studies or infer similar risk of injury at an individual level between conditions. For instance, O'Malley, Murphy performed the LESS barefoot.¹⁴ Their results would likely be comparable if performed with shoes in terms of the group mean LESS score and proportion of high injury-risk individuals, but the individual-level risk categorization might differ. Furthermore, the predictive value of the LESS performed barefoot for noncontact ACL injury has not been researched. Hence, when using the LESS in a clinical setting, test parameters should be kept constant for a given

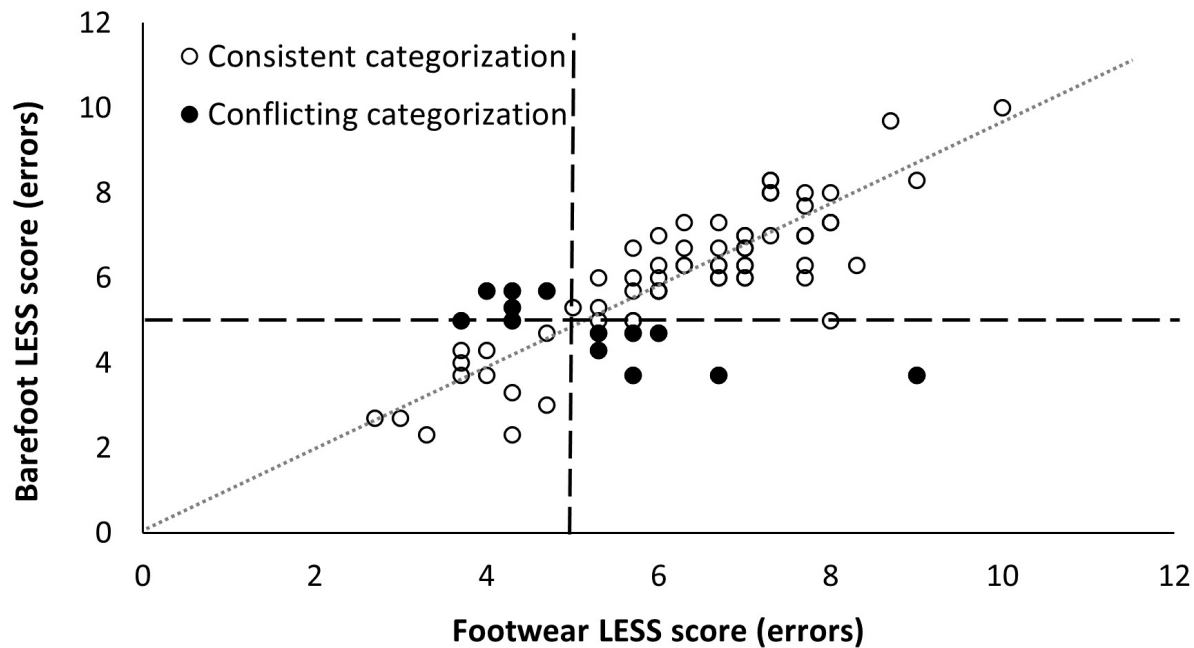


Figure 2. Landing Error Scoring System (LESS) score plots for both footwear and barefoot conditions for all 80 participants. The dashed grey dotted line represents the identity line. The dashed black lines represent the 5-error threshold that defines high (≥ 5 errors) and low (< 5 errors) injury risk.

Table 3. Landing Error Scoring System (LESS) specific errors for 80 participants.

No.	Items	Number of errors (% participants)		<i>p</i> -value*
		Footwear	Barefoot	
1	Knee flexion at initial contact	57 (71.3%)	50 (62.5%)	0.118
2	Hip flexion at initial contact	0 (0%)	0 (0%)	1.000
3	Trunk flexion at initial contact	1 (1.3%)	0 (0%)	1.000
4	Ankle plantar flexion at initial contact	14 (17.5%)	4 (5.0%)	0.006[†]
5	Knee valgus at initial contact	69 (86.3%)	59 (73.8%)	0.012[†]
6	Lateral trunk flexion at initial contact	6 (7.5%)	8 (10.0%)	0.688
7	Stance width (wide) at initial contact	12 (15.0%)	11 (13.8%)	1.000
8	Stance width (narrow) at initial contact	25 (31.3%)	32 (40.0%)	0.039[†]
9	Foot position (toe-in)	0 (0%)	1 (1.3%)	1.000
10	Foot position (toe-out)	12 (15.0%)	26 (32.5%)	0.003[†]
11	Symmetric foot contact at initial contact	53 (66.3%)	52 (65.0%)	1.000
12	Knee flexion at maximal knee flexion	5 (6.3%)	5 (6.3%)	1.000
13	Hip flexion at maximal knee flexion	1 (1.3%)	1 (1.3%)	1.000
14	Trunk flexion at maximal knee flexion	3 (3.8%)	2 (2.5%)	1.000
15	Knee valgus displacement	60 (75.0%)	56 (70.0%)	0.289
16	Joint displacement	55 (68.8%)	58 (72.5%)	0.581
17	Overall impression	76 (95.0%)	70 (87.5%)	0.109

Note. *Significant difference between conditions ($p \leq 0.05$) are in bold. [†]McNemar's test *p*-values for differences between conditions.

individual on separate occasions and the use of footwear is recommended given that it has demonstrated predictive value in youth.⁵ Most ACL injuries that occur during sports and recreational activities probably involve individuals

wearing their own athletic footwear; hence, performing the LESS with shoes is arguably more ecologically valid.

In biomechanics research, relying solely on null hypothesis significance testing without use of appropriate effect sizes or consideration of the magnitude of the difference is

discouraged.²⁶ It has been proposed that a one error change in LESS score is clinically meaningful.^{4,8} In fact, the inter-session standard error of measurement for the LESS is 0.81 error,²⁷ which exceeds the observed difference of 0.3 errors between footwear and barefoot conditions. Hence, although the difference between conditions reached statistical significance, the effect of footwear on overall mean LESS scores is not clinically meaningful. Despite this, differences of one error or more were observed in 33.8% of individuals and changes in injury risk categorization in 16.3% of individuals between footwear and barefoot conditions, again supporting use of a consistent footwear or barefoot protocol for a given individual when assessing injury risk or movement strategies over time.

The odds of errors significantly differed between footwear and barefoot conditions for four LESS items: knee valgus, ankle plantar flexion, narrow stance width, and toe-out foot position at initial contact (Items 4, 5, 8, and 10). The two first errors were 12.5% more prevalent in footwear, whereas the latter two were 8.7% and 17.5% less prevalent. Arguably, though, differences less than 10% are likely trivial in nature (i.e., narrow stance width).²⁸ Hanzlíková and Hébert-Losier⁹ also found that these specific LESS errors differed between self-selected and 50% body height landing conditions, alongside knee valgus displacement (Item 15). Furthermore, review of the running literature indicate that footwear influences knee, ankle, and stride kinematics.¹⁹ A heel-to-toe drop of zero, for instance, is more commonly associated with a forefoot strike pattern in running studies compared to running in footwear with a drop of 8 mm or more.²⁹ These findings combined suggest these specific LESS errors (Items 4, 5, 8, and 10) are more sensitive to change and alterations in protocol and footwear than the other errors. The differences in likelihood of specific LESS errors between footwear and barefoot conditions indicate differences in multi-joint strategies used to moderate impact forces during landing tasks, as shown elsewhere.¹¹ Barefoot, participants were more likely to land with greater ankle plantar flexion and the front part of their foot. These observations are comparable to findings of a more plantar-flexed ankle and greater foot-ground angle at initial contact from a 30-cm DLJL task similar to the LESS when performed barefoot compared to with shoes.¹² Landing in greater ankle plantar flexion during DLJL likely shifts loading between joints, with greater ankle but lesser knee joint loading. Indeed, participants with an ACL reconstruction landed from a 60-cm drop with greater ankle plantar flexion and absorbed a greater amount of force at the ankle compared to non-injured controls, presumably to protect their injured knee.³⁰ Furthermore, research also indicates that single-leg landing with greater ankle plantar flexion from a drop jump increases total energy dissipation and reduces peak vertical loading rates.³¹ Since landing in greater plantar flexion may reduce the risk of knee and hip injuries, DLJL barefoot may be considered as a training tool in the early stages of ACL injury rehabilitation to reduce knee loads and peak vertical loading rates. In addition, our data indicate that maximal jump performance is not compromised barefoot,

which is often of concern to coaches, clinicians, and athletes.

Although knee valgus at initial contact was one of the most frequent errors in both footwear and barefoot conditions, this error was 12.5% more prevalent in footwear. Previous research has identified knee valgus as a risk factor for ACL injury.^{32,33} Hewett, Myer tracked 205 female adolescent athletes over 13 months: nine sustained ACL injuries.³² These nine athletes all exhibited increased knee valgus when performing drop vertical jumps pre-injury. Therefore, this metric alone in the context of the LESS might suggest an increased ACL injury risk when wearing footwear compared to barefoot. However, knee valgus alone does not cause ACL injury.¹ ACL injuries are moreover linked with multi-planar mechanisms,³ often with a hyperextended or slightly flexed knee undergoing a valgus motion with either internal or external rotation.³⁴ Despite overt methodological limitations,³⁵ more recent research continues to challenge that knee valgus during drop jumps is a valid predictor of ACL injury, with no association between 2D frontal plane knee and hip motion during drop jumps and noncontact ACL injuries.³⁶

In the current study, a threshold of five or more errors was used to categorize participants at high injury risk based on previous research.⁵ However, the predictive value of the LESS is debated in research given other studies indicating a lack of association between LESS scores and noncontact ACL injury.³⁷ Noteworthy is that in these two studies,^{5, 37} photographs of participants suggest performance of the LESS in shoes in one study⁵ and barefoot in the other,³⁷ which might have influenced LESS scores at an individual level. The five-error threshold may be appropriate in footwear only. Furthermore, there is no population-specific LESS cut-off score established in the literature. For instance, there is a tendency in the literature for higher LESS scores in younger individuals.⁸ Hence, it remains to confirm whether the five-error threshold established from youth elite soccer players (age: 13.9 ± 1.8 y)⁵ apply to young active adults like those in the current study (age: 20.0 ± 2.3 y) in whom the LESS is often used.^{6,9,10,14,27,37} The mean LESS scores in this study are within the range of those reported for non-injured active young adults across the scientific literature.⁸ Nonetheless, over 75% of participants were categorized as high risk, which could reflect the inappropriateness of the 5-error threshold in this cohort or the fact that most participants were not involved in jump-landing sports. Non-contact ACL injuries are multifactorial in nature, with the LESS examining gross movement patterns only. It is also worth noting that a series of studies suggest that the vertical drop jump and DLJL tasks are poor predictors of future ACL injury.³⁸⁻⁴⁰ Out of five biomechanical variables examined across these studies (knee valgus angle at initial contact, peak knee abduction moment, peak knee flexion angle, peak vertical ground reaction force, and medial knee displacement), only medial knee displacement during the drop vertical jump was linked to ACL injuries prospectively, but sensitivity (0.6) and specificity (0.6) were poor.³⁸ In recent investigations, the ability to control the knees in the frontal plane during

landing from a DLJL was unable to distinguish between athletes who sustained an ACL injury to those who remained uninjured.⁴⁰ Despite these findings, DLJL tasks can still be useful as part of neuromuscular training programs for reducing ACL injury incidence⁴¹ and guiding rehabilitation or return-to-sport decision making post ACL reconstruction.^{6, 42} The LESS can also be useful for monitoring the effectiveness of programs and changes in biomechanical patterns.⁴³ Performing the DLJL in footwear and barefoot likely involves different multi-joint strategies, loads, and muscle recruitment and activation patterns, which might ultimately lead to different adaptations. As such, performing DLJL tasks in both footwear and barefoot within neuromuscular training programs could provide different stimuli to individuals. Given that participants wearing minimal footwear were excluded, the generalization of the current findings comparing DLJL measures between barefoot and different types of footwear needs confirmation.

CONCLUSION

Overall LESS scores were significantly greater and jump heights were significantly lower in footwear than barefoot, but differences were *trivial* and not clinically meaningful. At the group level, the proportion of participants categorized at high risk of injury was comparable between conditions; however, differences in specific landing errors, inconsistency in injury risk categorization, and clinically meaningful changes in LESS scores at an individual level were noted.

In clinical settings or for screening purposes, performing the LESS with shoes is still recommended given that the predictive value of the LESS barefoot has not been established. If the DLJL is used in neuromuscular training programs, performing the task both with and without shoes can offer variety in landing strategies and potentially different stimuli and neuromuscular adaptations to individuals.

CONFLICTS OF INTEREST STATEMENT

The authors report no conflicts of interest.

DATA AVAILABILITY

The data that support the findings of this study are openly available in OSF at <https://doi.org/10.17605/OSF.IO/KHS7V>.⁴⁴

ACKNOWLEDGMENTS

The authors thank Dr. Shannon O'Donnell and Mr. Dalton Berry for their assistance during the data collection process. The authors also thank the participants for their voluntary participation.

Submitted: October 28, 2022 CDT, Accepted: May 06, 2023 CDT



This is an open-access article distributed under the terms of the Creative Commons Attribution 4.0 International License (CCBY-NC-4.0). View this license's legal deed at <https://creativecommons.org/licenses/by-nc/4.0> and legal code at <https://creativecommons.org/licenses/by-nc/4.0/legalcode> for more information.

REFERENCES

1. Yu B, Garrett WE. Mechanisms of non-contact ACL injuries. *Br J Sports Med*. 2007;41(Supplement 1):i47-i51. [doi:10.1136/bjism.2007.037192](https://doi.org/10.1136/bjism.2007.037192)
2. Waldén M, Atroshi I, Magnusson H, Wagner P, Hägglund M. Prevention of acute knee injuries in adolescent female football players: Cluster randomised controlled trial. *BMJ*. 2012;344:e3042. [doi:10.1136/bmj.e3042](https://doi.org/10.1136/bmj.e3042)
3. Griffin LY, Albohm MJ, Arendt EA, et al. Understanding and preventing noncontact anterior cruciate ligament injuries: a review of the Hunt Valley II meeting, January 2005. *Am J Sports Med*. 2006;34(9):1512-1532. [doi:10.1177/0363546506286866](https://doi.org/10.1177/0363546506286866)
4. Padua DA, Marshall SW, Boling MC, Thigpen CA, Garrett WEJ, Beutler AI. The Landing Error Scoring System (LESS) is a valid and reliable clinical assessment tool of jump-landing biomechanics: The JUMP-ACL study. *Am J Sports Med*. 2009;37(10):1996-2002. [doi:10.1177/0363546509343200](https://doi.org/10.1177/0363546509343200)
5. Padua DA, DiStefano LJ, Beutler AI, de la Motte SJ, DiStefano MJ, Marshall SW. The Landing Error Scoring System as a screening tool for an anterior cruciate ligament injury-prevention program in elite-youth soccer athletes. *J Athl Train*. 2015;50(6):589-595. [doi:10.4085/1062-6050-50.1.10](https://doi.org/10.4085/1062-6050-50.1.10)
6. Bell DR, Smith MD, Pennuto AP, Stiffler MR, Olson ME. Jump-landing mechanics after anterior cruciate ligament reconstruction: A landing error scoring system study. *J Athl Train*. 2014;49(4):435-441. [doi:10.4085/1062-6050-49.3.21](https://doi.org/10.4085/1062-6050-49.3.21)
7. Hanzlíková I, Hébert-Losier K. Is the Landing Error Scoring System reliable and valid? A systematic review. *Sports Health*. 2020;12(2):181-188. [doi:10.1177/1941738119886593](https://doi.org/10.1177/1941738119886593)
8. Hanzlíková I, Athens J, Hébert-Losier K. Factors influencing the Landing Error Scoring System: Systematic review with meta-analysis. *J Sci Med Sport*. 2021;24(3):269-280. [doi:10.1016/j.jsams.2020.08.013](https://doi.org/10.1016/j.jsams.2020.08.013)
9. Hanzlíková I, Hébert-Losier K. Clinical implications of landing distance on Landing Error Scoring System scores. *J Athl Train*. 2021;56(6):572-577. [doi:10.4085/1062-6050-068-20](https://doi.org/10.4085/1062-6050-068-20)
10. Hanzlíková I, Athens J, Hébert-Losier K. Clinical implications of Landing Error Scoring System calculation methods. *Phys Ther Sport*. 2020;44:61-66. [doi:10.1016/j.pts.2020.04.035](https://doi.org/10.1016/j.pts.2020.04.035)
11. Shultz SJ, Schmitz RJ, Tritsch AJ, Montgomery MM. Methodological considerations of task and shoe wear on joint energetics during landing. *J Electromyogr Kinesiol*. 2012;22(1):124-130. [doi:10.1016/j.jelekin.2011.11.001](https://doi.org/10.1016/j.jelekin.2011.11.001)
12. Koyama K, Yamauchi J. Comparison of lower limb kinetics, kinematics and muscle activation during drop jumping under shod and barefoot conditions. *J Biomech*. 2018;69:47-53. [doi:10.1016/j.jbiomech.2018.01.011](https://doi.org/10.1016/j.jbiomech.2018.01.011)
13. Yeow CH, Lee PVS, Goh JCH. Shod landing provides enhanced energy dissipation at the knee joint relative to barefoot landing from different heights. *Knee*. 2011;18(6):407-411. [doi:10.1016/j.knee.2010.07.011](https://doi.org/10.1016/j.knee.2010.07.011)
14. O'Malley E, Murphy JC, Persson UM, Gissane C, Blake C. The effects of the gaelic athletic association 15 training program on neuromuscular outcomes in gaelic football and hurling players: a randomized cluster trial. *J Strength Cond Res*. 2017;31(8):2119-2130. [doi:10.1519/jsc.0000000000001564](https://doi.org/10.1519/jsc.0000000000001564)
15. LaPorta JW, Brown LE, Coburn JW, et al. Effects of different footwear on vertical jump and landing parameters. *J Strength Cond Res*. 2013;27(3):733-737. [doi:10.1519/jsc.0b013e318280c9ce](https://doi.org/10.1519/jsc.0b013e318280c9ce)
16. Esculier JF, Dubois B, Dionne CE, Leblond J, Roy JS. A consensus definition and rating scale for minimalist shoes. *J Foot Ankle Res*. 2015;8(1):1-9. [doi:10.1186/s13047-015-0094-5](https://doi.org/10.1186/s13047-015-0094-5)
17. Fuller JT, Thewlis D, Tsiros MD, Brown NAT, Buckley JD. Six-week transition to minimalist shoes improves running economy and time-trial performance. *J Sci Med Sport*. 2017;20(12):1117-1122. [doi:10.1016/j.jsams.2017.04.013](https://doi.org/10.1016/j.jsams.2017.04.013)
18. Squadrone R, Rodano R, Hamill J, Preatoni E. Acute effect of different minimalist shoes on foot strike pattern and kinematics in rearfoot strikers during running. *J Sports Sci*. 2015;33(11):1196-1204. [doi:10.1080/02640414.2014.989534](https://doi.org/10.1080/02640414.2014.989534)

19. Hall JPL, Barton C, Jones PR, Morrissey D. The biomechanical differences between barefoot and shod distance running: A systematic review and preliminary meta-analysis. *Sports Med.* 2013;43(12):1335-1353. [doi:10.1007/s40279-013-0084-3](https://doi.org/10.1007/s40279-013-0084-3)
20. Malisoux L, Gette P, Urhausen A, Bomfim J, Theisen D. Influence of sports flooring and shoes on impact forces and performance during jump tasks. *PLoS One.* 2017;12(10):e0186297. [doi:10.1371/journal.pone.0186297](https://doi.org/10.1371/journal.pone.0186297)
21. Craig CL, Marshall AL, Sjöström M, et al. International physical activity questionnaire: 12-country reliability and validity. *Med Sci Sports Exerc.* 2003;35(8):1381-1395. [doi:10.1249/01.mss.0000078924.61453.fb](https://doi.org/10.1249/01.mss.0000078924.61453.fb)
22. Hanzlíková I, Hébert-Losier K. Landing Error Scoring System scores change with knowledge of scoring criteria and prior performance. *Phys Ther Sport.* 2020;46:155-161. [doi:10.1016/j.ptsp.2020.09.004](https://doi.org/10.1016/j.ptsp.2020.09.004)
23. Linthorne NP. Analysis of standing vertical jumps using a force platform. *Am J Phys.* 2001;69(11):1198-1204. [doi:10.1119/1.1397460](https://doi.org/10.1119/1.1397460)
24. Cohen J. *Statistical Power Analysis for the Behavioral Sciences*. 2nd revised ed. Routledge; 2013. [doi:10.4324/9780203771587](https://doi.org/10.4324/9780203771587)
25. Gallardo-Fuentes F, Gallardo-Fuentes J, Ramírez-Campillo R, et al. Intersession and intrasession reliability and validity of the My Jump App for measuring different jump actions in trained male and female athletes. *J Strength Cond Res.* 2016;30(7):2049-2056. [doi:10.1519/jsc.0000000000001304](https://doi.org/10.1519/jsc.0000000000001304)
26. Harrison AJ, McErlain-Naylor SA, Bradshaw EJ, et al. Recommendations for statistical analysis involving null hypothesis significance testing. *Sports Biomech.* 2020;19(5):561-568. [doi:10.1080/14763141.2020.1782555](https://doi.org/10.1080/14763141.2020.1782555)
27. Scarneo SE, Root HJ, Martinez JC, et al. Landing technique improvements after an aquatic-based neuromuscular training program in physically active women. *J Sport Rehabil.* 2017;26(1):8-14. [doi:10.1123/jsr.2015-0052](https://doi.org/10.1123/jsr.2015-0052)
28. Hopkins WG, Marshall SW, Batterham AM, Hanin J. Progressive statistics for studies in sports medicine and exercise science. *Med Sci Sports Exerc.* 2009;41(1):3-12. [doi:10.1249/mss.0b013e31818cb278](https://doi.org/10.1249/mss.0b013e31818cb278)
29. Sánchez-Ramírez C, Ramsey C, Palma-Oyarce V, Herrera-Hernández E, Aedo-Muñoz E. Heel-to-toe drop of running shoes: A systematic review of its biomechanical effects. *Footwear Sci.* 2023;2023:1-25. [doi:10.1080/19424280.2023.2180542](https://doi.org/10.1080/19424280.2023.2180542)
30. Decker MJ, Torry MR, Noonan TJ, Riviere A, Sterett WI. Landing adaptations after ACL reconstruction. *Med Sci Sports Exerc.* 2002;34(9):1408-1413. [doi:10.1097/00005768-200209000-00002](https://doi.org/10.1097/00005768-200209000-00002)
31. Lee J, Song Y, Shin CS. Effect of the sagittal ankle angle at initial contact on energy dissipation in the lower extremity joints during a single-leg landing. *Gait Posture.* 2018;62:99-104. [doi:10.1016/j.gaitpost.2018.03.019](https://doi.org/10.1016/j.gaitpost.2018.03.019)
32. Hewett TE, Myer GD, Ford KR, et al. Biomechanical measures of neuromuscular control and valgus loading of the knee predict anterior cruciate ligament injury risk in female athletes: A prospective study. *Am J Sports Med.* 2005;33(4):492-501. [doi:10.1177/0363546504269591](https://doi.org/10.1177/0363546504269591)
33. McLean SG, Huang X, van den Bogert AJ. Association between lower extremity posture at contact and peak knee valgus moment during sidestepping: implications for ACL injury. *Clin Biomech.* 2005;20(8):863-870. [doi:10.1016/j.clinbiomech.2005.05.007](https://doi.org/10.1016/j.clinbiomech.2005.05.007)
34. Shimokochi Y, Shultz SJ. Mechanisms of noncontact anterior cruciate ligament injury. *J Athl Train.* 2008;43(4):396-408. [doi:10.4085/1062-6050-43.4.396](https://doi.org/10.4085/1062-6050-43.4.396)
35. Russo L, Padulo J, Oliva F, Maffulli N. Letter to Editor about 'Kiss goodbye to the "kissing knees": No association between frontal plane inward knee motion and risk of future non-contact ACL injury in elite female athletes.' *Sports Biomech.* 2021;2021:1-3. [doi:10.1080/14763141.2021.1968024](https://doi.org/10.1080/14763141.2021.1968024)
36. Nilstad A, Petushek E, Mok KM, Bahr R, Krosshaug T. Kiss goodbye to the 'kissing knees': No association between frontal plane inward knee motion and risk of future non-contact ACL injury in elite female athletes. *Sports Biomech.* 2023;22(1):65-79. [doi:10.1080/14763141.2021.1903541](https://doi.org/10.1080/14763141.2021.1903541)
37. Smith HC, Johnson RJ, Shultz SJ, et al. A prospective evaluation of the Landing Error Scoring System (LESS) as a screening tool for anterior cruciate ligament injury risk. *Am J Sports Med.* 2012;40(3):521-526. [doi:10.1177/0363546511429776](https://doi.org/10.1177/0363546511429776)

38. Krosshaug T, Steffen K, Kristianslund E, et al. The vertical drop jump is a poor screening test for ACL injuries in female elite soccer and handball players: A prospective cohort study of 710 athletes. *Am J Sports Med.* 2016;44(4):874-883. [doi:10.1177/0363546515625048](https://doi.org/10.1177/0363546515625048)
39. Mørtned AI, Krosshaug T, Bahr R, Petushek E. I spy with my little eye ... a knee about to go 'pop'? Can coaches and sports medicine professionals predict who is at greater risk of ACL rupture? *Br J Sports Med.* 2020;54(3):154-158. [doi:10.1136/bjsports-2019-100602](https://doi.org/10.1136/bjsports-2019-100602)
40. Petushek E, Nilstad A, Bahr R, Krosshaug T. Drop jump? Single-leg squat? Not if you aim to predict anterior cruciate ligament injury from real-time clinical assessment: a prospective cohort study involving 880 elite female athletes. *J Orthop Sports Phys Ther.* 2021;51(7):372-378. [doi:10.2519/jospt.2021.10170](https://doi.org/10.2519/jospt.2021.10170)
41. Myer GD, Ford KR, Brent JL, Hewett TE. Differential neuromuscular training effects on ACL injury risk factors in "high-risk" versus "low-risk" athletes. *BMC Musculoskelet Disord.* 2007;8(1):1-7. [doi:10.1186/1471-2474-8-39](https://doi.org/10.1186/1471-2474-8-39)
42. Welling W, Benjaminse A, Seil R, Lemmink K, Zaffagnini S, Gokeler A. Low rates of patients meeting return to sport criteria 9 months after anterior cruciate ligament reconstruction: A prospective longitudinal study. *Knee Surg Sports Traumatol Arthrosc.* 2018;26(12):3636-3644. [doi:10.1007/s00167-018-4916-4](https://doi.org/10.1007/s00167-018-4916-4)
43. Garbenytė-Apolinskienė T, Šiupšinskas L, Salatkaitė S, Gudas R, Radvila R. The effect of integrated training program on functional movements patterns, dynamic stability, biomechanics, and muscle strength of lower limbs in elite young basketball players. *Sport Sci Health.* 2018;14(2):245-250. [doi:10.1007/s11332-017-0409-y](https://doi.org/10.1007/s11332-017-0409-y)
44. Hébert-Losier K. Landing Error Scoring System footwear dataset. OSF. Published online October 24, 2022. [doi:10.17605/OSF.IO/KHS7V](https://doi.org/10.17605/OSF.IO/KHS7V)